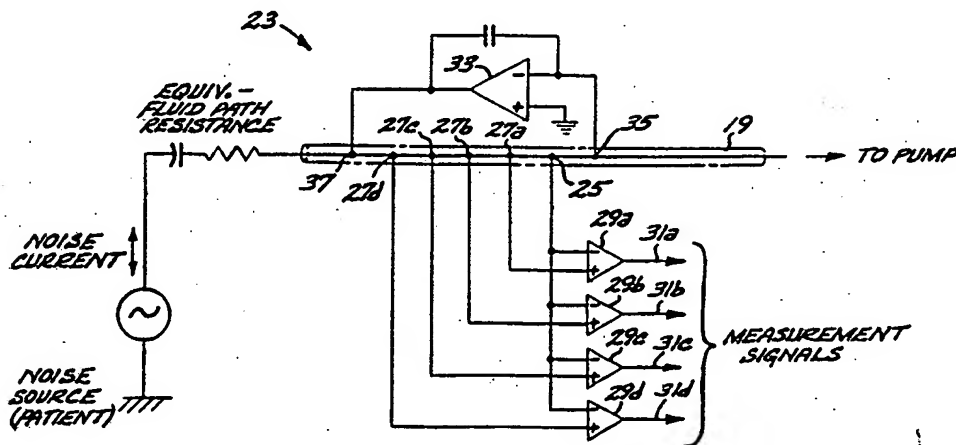


PCT

WORLD INTELLECTUAL PROPERTY ORGANIZATION  
International Bureau

## INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

|   |           |  |
|---|-----------|--|
| <b>(51) International Patent Classification <sup>5</sup> :</b><br><br><b>G01N 33/49, 27/26</b>  | <b>A1</b> | <b>(11) International Publication Number:</b> <b>WO 93/09433</b><br><br><b>(43) International Publication Date:</b> <b>13 May 1993 (13.05.93)</b>  |
| <b>(21) International Application Number:</b> PCT/US92/09678<br><b>(22) International Filing Date:</b> 9 November 1992 (09.11.92)<br><br><b>(30) Priority data:</b><br>790,669                      8 November 1991 (08.11.91)    US<br><br><b>(71) Applicant:</b> VIA MEDICAL CORPORATION [US/US];<br>10633 Roselle Street, San Diego, CA 92121 (US).<br><b>(72) Inventor:</b> GHARIB, James, E. ; 6725 Greenbrier Court,<br>San Diego, CA 92120 (US).<br><br><b>(74) Agent:</b> BRUEGGEMANN, James, R.; Pretty, Schroeder,<br>Brueggemann & Clark, 444 South Flower Street, Suite<br>2000, Los Angeles, CA 90071-2921 (US). |           | <b>(81) Designated States:</b> DE, GB, JP, European patent (AT, BE, CH, DE, DK, ES, FR, GB, GR, IE, IT, LU, MC, NL, SE).<br><br><b>Published</b><br><i>With international search report.<br/>         Before the expiration of the time limit for amending the claims and to be republished in the event of the receipt of amendments.</i> |

**(54) Title:** ELECTROCHEMICAL MEASUREMENT SYSTEM HAVING INTERFERENCE REDUCTION CIRCUIT**(57) Abstract**

A system for electrically measuring certain chemical characteristics of electrically-conductive fluids, such as blood, located within a tube and subject to electrical current interference. The measurements are made by measuring the voltage potential between a reference electrode and a sensor electrode sensitive to a particular blood parameter such as pH or calcium, potassium or chloride concentration. A bypass path for the electrical current interference is provided by a pair of noise-reduction electrodes located on opposite sides of the reference and sensor electrodes and interconnected by an amplifier having a relatively low output impedance and a relatively high input impedance. The electrical current interference bypasses the signal electrodes by flowing directly into the amplifier's output terminal, such that the reference and sensor electrodes develop a potential between them that is independent of the electrical current interference.

BEST AVAILABLE COPY

**FOR THE PURPOSES OF INFORMATION ONLY**

Codes used to identify States party to the PCT on the front pages of pamphlets publishing international applications under the PCT.

|    |                          |    |                                       |    |                          |
|----|--------------------------|----|---------------------------------------|----|--------------------------|
| AT | Austria                  | FR | France                                | MR | Mauritania               |
| AU | Australia                | GA | Gabon                                 | MW | Malawi                   |
| BB | Barbados                 | GB | United Kingdom                        | NL | Netherlands              |
| BE | Belgium                  | GN | Guinea                                | NO | Norway                   |
| BF | Burkina Faso             | GR | Greece                                | NZ | New Zealand              |
| BG | Bulgaria                 | HU | Hungary                               | PL | Poland                   |
| BJ | Benin                    | IE | Ireland                               | PT | Portugal                 |
| BR | Brazil                   | IT | Italy                                 | RO | Romania                  |
| CA | Canada                   | JP | Japan                                 | RU | Russian Federation       |
| CF | Central African Republic | KP | Democratic People's Republic of Korea | SD | Sudan                    |
| CG | Congo                    | KR | Republic of Korea                     | SE | Sweden                   |
| CH | Switzerland              | KZ | Kazakhstan                            | SK | Slovak Republic          |
| CI | Côte d'Ivoire            | LJ | Liechtenstein                         | SN | Senegal                  |
| CM | Cameroon                 | LK | Sri Lanka                             | SU | Soviet Union             |
| CS | Czechoslovakia           | LU | Luxembourg                            | TD | Chad                     |
| CZ | Czech Republic           | MC | Monaco                                | TG | Togo                     |
| DE | Germany                  | MG | Madagascar                            | UA | Ukraine                  |
| DK | Denmark                  | ML | Mali                                  | US | United States of America |
| ES | Spain                    | MN | Mongolia                              | VN | Viet Nam                 |
| FI | Finland                  |    |                                       |    |                          |

ELECTROCHEMICAL MEASUREMENT SYSTEM  
HAVING INTERFERENCE REDUCTION CIRCUIT

BACKGROUND OF THE INVENTION

This invention relates generally to systems for electrically measuring certain chemical characteristics of fluids, e.g., concentration of certain analytes such as ions, gases and metabolites in human blood, and, more particularly, to electrical circuits for reducing the effects of electrical interference in such measurement systems.

Systems of this general kind can take the form of blood chemistry diagnostic systems integrated into infusion fluid delivery systems of the kind commonly used in hospital patient care. Such fluid delivery systems infuse nutrients, medications and the like directly into the patient at a controlled rate and in precise quantities for maximum effectiveness. Infusion fluid delivery systems are connected to a patient at an intravenous (IV) port, in which a hollow needle/catheter combination is inserted into a blood vessel of the patient and thereafter an infusion fluid is introduced into the vessel at a controlled rate, typically using a peristaltic pump. Blood chemistry monitoring systems that are combined with infusion delivery systems of this kind use the IV port to periodically withdraw a blood sample, perform measurements of blood ion concentrations and the like, and then discard the blood or reinfuse it into the patient. The system then resumes delivery of the infusion fluid.

Such combined infusion fluid delivery and blood chemistry monitoring systems include an infusion line and catheter through which the infusion fluid is provided to the patient and blood samples are withdrawn. The infusion line incorporates an electrode assembly having electrochemical sensors that are periodically exposed to

the blood samples and thereby provide electrical signals to an analyzer for conversion into corresponding blood chemistry data. A control unit periodically halts delivery of the infusion fluid for a brief interval, during which time a blood sample is withdrawn from the patient into the infusion line and routed to the electrode assembly, which then generates the electrical signals. After the electrical signals have been received by the analyzer, the control unit disposes of the blood or reinfuses it into the patient, and the flow of infusion fluid is resumed.

The electrode assembly typically includes a reference electrode and a plurality of sensor electrodes that are each sensitive to a particular ion of interest. All of the electrodes are embedded in the base of the electrode assembly. Electrochemical sensors generate electrical signals, either a voltage or a current, only in response to contact with the particular species to which they are sensitive, and therefore provide selective measurement of the amount of that species in the blood. Sensor electrodes can be provided to measure, for example, partial pressure of oxygen ( $pO_2$ ) and carbon dioxide ( $pCO_2$ ), glucose, calcium, hydrogen ion, chloride, potassium, and sodium.

The accuracy of the measurements described above can be adversely affected by any electrical current interference, usually originating at the patient, that is conducted along the infusion tube by the blood and the infusion fluid. Appropriate low-pass filtering of the electrical potential measurements can reduce the effects of this noise; however, substantial inaccuracies remain. Movement of the infusion tube relative to the patient provides even greater noise and makes the task of filtering or otherwise reducing the effects of the noise even more difficult.

It should therefore be appreciated that there is a need for an electrochemical measurement system of this particular kind that is less susceptible to interference from electrical current noise being conducted along the fluid line. The present invention fulfills this need.

#### SUMMARY OF THE INVENTION

This invention resides in an apparatus, and related method, for measuring a predetermined parameter of an electrically-conductive fluid located in a tube, which are effective in substantially eliminating the adverse effects of any electrical current interference being conducted along the tube from a noise source at one end of the tube. The apparatus and method are particularly useful as part of an infusion delivery system, in analyzing of blood chemistry.

More particularly, the apparatus includes an electrode assembly having a reference electrode and a plurality of sensor electrodes located at spaced-apart locations along a fluid path, along with signal amplifier means for sensing the voltage between the reference electrode and each sensor electrode and for providing a corresponding voltage signal indicative of a predetermined parameter of the contained fluid, for which the particular sensor is sensitive. The sensor electrodes can include ion-selective electrodes and other types of electrochemical sensors. First and second noise-reduction electrodes also are located in the electrode assembly, on opposite sides of the reference and sensor electrodes. A noise-reduction amplifier having an input terminal with a high impedance and an output terminal with a low impedance is connected between the first and second noise-reduction electrodes, with its input terminal connected to the electrode furthest from the noise source and with its

output terminal connected to the electrode closest to the noise source. Electrical current interference thereby is diverted through the noise-reduction amplifier, bypassing the portion of the infusion tube where the reference and sensor electrodes are located. The voltage signals produced by the signal amplifier means thereby are substantially unaffected by that electrical current interference.

10 In other, more detailed features of the invention, the noise-reduction amplifier takes the form of an operational amplifier with its negative input terminal connected to the noise-reduction electrode located furthest from the noise source and with its positive input terminal connected to a ground reference. The electrical current interference typically is only ac, and the noise-reduction amplifier is operable to bypass the entire bandwidth of the ac current.

20 Other features and advantages of this invention should become apparent from the following description of the preferred embodiment, taken in conjunction with the accompanying drawings, which illustrate, by way of example, the principles of the invention.

#### BRIEF DESCRIPTION OF THE DRAWINGS

25 FIG. 1 is a schematic diagram of a combination infusion fluid delivery and blood chemistry analysis system in accordance with a preferred embodiment of the invention, shown being coupled to the arm of a patient.

30 FIG. 2 is a schematic circuit diagram of an electrode/amplifier assembly having a noise-reduction circuit, the assembly being part of the analysis system of FIG. 1.

FIG. 2A is a schematic circuit diagram of one equivalent circuit for each electrode in the electrode/amplifier assembly of FIG. 2.

FIG. 2B is a schematic circuit diagram of an alternative equivalent circuit for each electrode in the electrode/amplifier assembly of FIG. 2.

#### DESCRIPTION OF THE PREFERRED EMBODIMENT

The following description of the preferred embodiment of the invention is not to be taken in a limiting sense, but is made merely for the purpose of illustrating the general principles of the invention. The description is of the best mode presently contemplated for carrying out the invention.

With reference to FIG. 1, there is shown an infusion fluid delivery and blood chemistry analysis system in use connected to the arm 11 of a patient. An infusion pump 13, under the control of a controller 15, pumps an infusion fluid from a fluid source 17 to a blood vessel in the patient's arm via an infusion tube 19 and hollow needle 21. An electrode assembly 23 is located in the middle of the infusion line and arranged such that the infusion fluid passes through it on its way to the patient.

Periodically, the controller 15 conditions the pump 13 to interrupt its pumping of the infusion fluid to the patient and, instead, to reverse direction and draw a blood sample from the patient. This blood sample is drawn rearwardly through the infusion tube 19 as far as the electrode assembly 23, to allow the assembly to measure certain characteristics of the blood. After the measurements have been completed, the pump reinfuses the blood sample back into the patient, and then resumes

pumping the infusion fluid.

The electrode assembly 23 is depicted in greater detail in FIG. 2. It includes a single reference electrode 25 and four separate sensor electrodes 27a-27d located at spaced location along the fluid flow path and arranged to contact the fluid flowing through it. Each of the sensor electrodes includes an electrochemical sensor and it is adapted to develop between it and the reference electrode a voltage potential that varies in accordance with a predetermined parameter of the adjacent fluid to which the electrochemical sensor is sensitive. Examples of parameters that are commonly measured in this fashion include pH, concentrations of sodium, potassium and calcium, and glucose, hematocrit, and partial pressures of oxygen ( $pO_2$ ) and carbon dioxide ( $pCO_2$ ). Amplifiers 29a-29d are arranged to amplify the differential voltages provided by the reference electrode and the respective sensor electrodes 27a-27d, to provide amplified measurement signals for output on lines 31a-31d.

In blood chemistry analysis systems like that depicted in FIG. 1, it is known that electrical interference in the form of an undesired electrical current can originate at the patient and be conducted along the infusion tube 19 by the contained fluid, i.e., infusion fluid and/or blood, and thus can interfere with the potential measurements being made. This electrical current interference has only ac components and is affected substantially by movement of the patient and/or the infusion tube. The current affects the voltage potential measurements in accordance with the inherent resistivity of the fluid(s) located between the reference electrode 25 and each sensor electrode 27a-27d.

In accordance with the invention, a bypass path for the electrical current interference is provided by an



operational amplifier 33 connected between first and second noise-reduction electrodes 35 and 37, respectively, situated on opposite sides of the reference electrode 25 and the plurality of sensor electrodes 27a-27d. One  
5 suitable form for the electrode assembly is described in detail in copending, commonly-assigned U.S. patent application Serial No. 07/581,803, filed in the name of David K. Wong and entitled "Electrochemical Sensor Apparatus and Method," which is incorporated by reference.  
10 In particular, the operational amplifier's negative, or inverting, input terminal is connected to the noise-reduction electrode 35 located furthest from the patient, while the amplifier's output terminal is connected to the noise-reduction electrode 37 located closest to the  
15 patient. The amplifier's positive, or non-inverting, input terminal is connected to a ground reference.

As is conventional, the operational amplifier 33 has a relatively high input impedance that is many orders of magnitude greater than its relatively low output  
20 impedance. Consequently, noise currents originating at the patient and flowing along the electrically-conductive fluid in the infusion tube 19 to the electrode assembly 23 are readily diverted to the operational amplifier's output terminal, which functions much like a current sink. The  
25 current thereby is precluded from flowing along the fluid located between each signal electrode 27a-27d and the reference electrode 25. The voltage measurements made between these electrodes thereby are substantially unaffected by this electrical current interference  
30 originating at the patient.

The noise-reduction electrodes 35 and 37 can be of any suitable construction. Preferably, the first noise-reduction electrode 35 takes the form of a bare silver, silver-plated steel, or stainless steel pin in  
35 direct contact with the infusion fluid. The second noise-

reduction electrode 37 may be of similar construction or may take the form of an ion-sensitive electrode, e.g., a sodium-sensitive electrode, like the sensor electrodes 27a-27d.

5           The reference electrode 25, the sensor electrodes 27a-27d, and the noise-reduction electrodes 35 and 37 typically are considered to have an equivalent electrical circuit in the form of a resistor 39 in series with a battery 41 of specified voltage. This is depicted  
10 in FIG. 2A.

The electrodes alternatively can be considered to have more complex equivalent circuits such as a parallel combination of a resistor 43 and capacitor 45 in series with a battery 47, as depicted in FIG. 2B.

15           In the case of the reference electrode and sensor electrodes 27a-27d, the batteries in the equivalent circuits yield dc voltage differences that are amplified by the amplifiers 29a-29d. The electrical current flowing through the electrodes is negligible, so the electrode  
20 resistance is of minimal significance. Further, the dc voltage differences provided by the noise-reduction electrodes 35 and 37 are of no concern, because the noise-reduction circuit functions merely as a bypass path for ac electrical current interference originating at the  
25 patient. A feedback capacitor 49 for the operational amplifier 33 limits the circuit's ac bandwidth to an appropriate range, to overcome the bandwidth of the noise signal.

30           It should be appreciated from the foregoing description that the present invention provides an improved system for electrically measuring certain chemical characteristics of electrically-conductive fluids such as blood located within a tube and subject to

electrical current interference. The measurements are made by measuring the voltage potential between a reference electrode and a sensor electrode located in the fluid line. A bypass path for the electrical current interference is provided by a pair of noise-reduction electrodes that are located on opposite sides of the reference and sensor electrodes and interconnected by an amplifier having a relatively low output impedance and a relatively high input impedance. In particular, the electrical current interference flows directly into the amplifier's output terminal, thereby ensuring that the reference and sensor electrodes develop a potential between them that is independent of the interference. Noise reductions on the order of 120db are readily achievable.

Although the invention has been described in detail with reference to the presently preferred embodiment, those of ordinary skill in the art will appreciate that various modifications can be made without departing from the invention. Accordingly, the invention is defined only by the following claims.

## Claims

10

1. Apparatus for measuring a predetermined parameter of an electrically-conductive fluid located in a tube and used in an environment where an undesired electrical current can be conducted by the fluid from a noise source at one end of the tube, the apparatus comprising:

a reference electrode and a sensor electrode adapted to be attached to a tube at spaced-apart locations, contacting an electrically-conductive fluid in the tube;

signal amplifier means for amplifying the voltage between the reference electrode and the sensor electrode and for providing a corresponding amplified signal;

first and second noise-reduction electrodes adapted to be attached to the tube at spaced-apart locations, contacting the electrically conductive fluid in the tube, such that the reference and sensor electrodes are located between the first and second noise-reduction electrodes; and

noise-reduction amplifier means having an input terminal with a high impedance and an output terminal with a low impedance, the noise-reduction amplifier means being connected between the first and second noise-reduction electrodes, with its input terminal connected to the noise-reduction electrode furthest from the noise source and with its output terminal connected to the noise-reduction electrode closest to the noise source, such that any electrical current originating at the noise source bypasses the portion of the electrically-conductive fluid located in the tube between the reference and sensor electrodes by flowing instead through the noise-reduction amplifier means, whereby the amplified signal produced by the signal amplifier means is substantially unaffected by that electrical current.

2. Apparatus as defined in claim 1, wherein the noise-reduction amplifier means includes an operational amplifier having a negative input terminal connected to the noise-reduction electrode that is furthest from the noise source, a positive input terminal  
5 connected to a ground reference, and an output terminal connected to the noise-reduction electrode that is closest to the noise source.

3. Apparatus as defined in claim 1, wherein:  
the apparatus further includes one or more additional sensor electrodes; and  
the signal amplifier means include a  
5 plurality of amplifiers, each amplifier for amplifying the voltage between the reference electrode and a separate sensor electrode and for providing a corresponding amplified signal.

4. Apparatus as defined in claim 1, wherein:  
the noise source generates an ac electrical current having a bandwidth; and  
the noise-reduction amplifier means is  
5 adapted to conduct the ac electrical current over the current's entire bandwidth.

5. Apparatus as defined in claim 1, wherein:  
the tube is connected at one end to a patient;  
the electrically-conductive fluid is blood;  
5 and  
the reference electrode and the sensor electrode are adapted to develop between them a voltage that is indicative of a predetermined parameter of the blood.

6. Apparatus as defined in claim 1, wherein the first and second noise-reduction electrodes are pins

formed of silver, silver-plated steel, or stainless steel.

7. Apparatus as defined in claim 1, wherein:  
the noise-reduction electrode located  
furthest from the noise source is a pin formed of silver,  
silver-plated steel, or stainless steel; and  
the noise-reduction electrode located  
5 closest to the noise source is sensitive to a  
predetermined parameter of the electrically-conductive  
fluid.

8. Apparatus for measuring a predetermined  
parameter of blood drawn from a patient into an  
intravenous tube, the apparatus comprising:  
a reference electrode and a sensor  
5 electrode adapted to be attached at spaced-apart locations  
in an intravenous tube into which blood can be drawn from  
a patient to contact the two electrodes, wherein a  
potential develops between the two electrodes that is  
indicative of a predetermined parameter of the blood;  
10 wherein electrical current interference  
originating at the patient can be conducted along the  
intravenous tube by blood contained in the tube;  
first and second noise-reduction electrodes  
adapted to be attached at spaced-apart locations in the  
15 intravenous tube, in contact with blood drawn into the  
tube, such that the reference and sensor electrodes are  
located between the first and second noise-reduction  
electrodes; and  
noise-reduction amplifier means having an  
20 input terminal with high impedance and an output terminal  
with a low impedance, the noise-reduction amplifier means  
being connected between the first and second noise-  
reduction electrodes, with the input terminal connected to  
the noise-reduction electrode furthest from the patient  
25 and with the output terminal connected to the noise-  
reduction electrode closest to the patient, such that any

electrical current originating at the patient bypasses the portion of the tube between the reference and sensor electrodes by flowing instead through the noise-reduction amplifier means, whereby the potential developed between the reference and sensor electrodes is substantially unaffected by that electrical current.

9. Apparatus as defined in claim 8, wherein the noise-reduction amplifier means includes an operational amplifier having a negative input terminal connected to the noise-reduction electrode that is furthest from the patient, a positive input terminal connected to a ground reference, and an output terminal connected to the noise-reduction electrode that is closest to the patient.

10. Apparatus as defined in claim 8, wherein: the electrical current noise originating at the patient is an ac current having a bandwidth; and the noise-reduction amplifier means is adapted to conduct the ac current over the current's entire bandwidth.

11. Apparatus as defined in claim 8, wherein the first and second noise-reduction electrodes are pins formed of silver, silver-plated steel, or stainless steel.

12. Apparatus as defined in claim 8, wherein: the noise-reduction electrode located furthest from the noise source is a pin formed of silver, silver-plated steel, or stainless steel; and the noise-reduction electrode located closest to the noise source is sensitive to a predetermined parameter of the electrically-conductive fluid.

13. A method for measuring a predetermined parameter of blood drawn from a patient into an intravenous tube, the method comprising steps of:

5 providing an electrode and infusion tube assembly having a reference electrode and a sensor electrode located at spaced apart locations, the sensor electrode being sensitive to a particular parameter of blood;

10 arranging the electrode and infusion tube assembly such that blood can be drawn from a patient into contact with one or both of the reference and sensor electrodes, wherein a potential develops between the two electrodes that is indicative of the predetermined parameter of the blood, and wherein electrical current  
15 interference originating at the patient can be conducted along the infusion tube by the blood contained in the tube; and

connecting a noise-reduction amplifier between two noise-reduction electrodes located on opposite  
20 sides of the reference and sensor electrodes, wherein the amplifier has a high-impedance input terminal connected to the noise reduction electrode located furthest from the patient and a low-impedance output terminal connected to the noise reduction electrode closest to the patient, such  
25 that any electrical current interference originating at the patient bypasses the reference and sensor electrodes by flowing instead through the noise-reduction amplifier, whereby the potential developed between the reference and sensor electrodes is substantially unaffected by that  
30 electrical current.



1/1

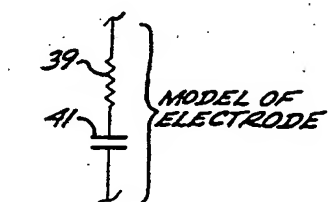
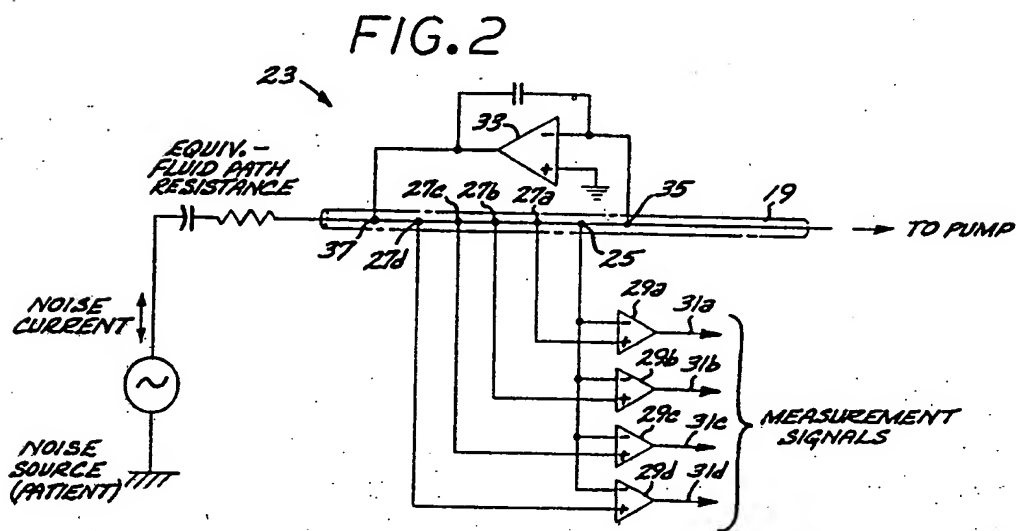
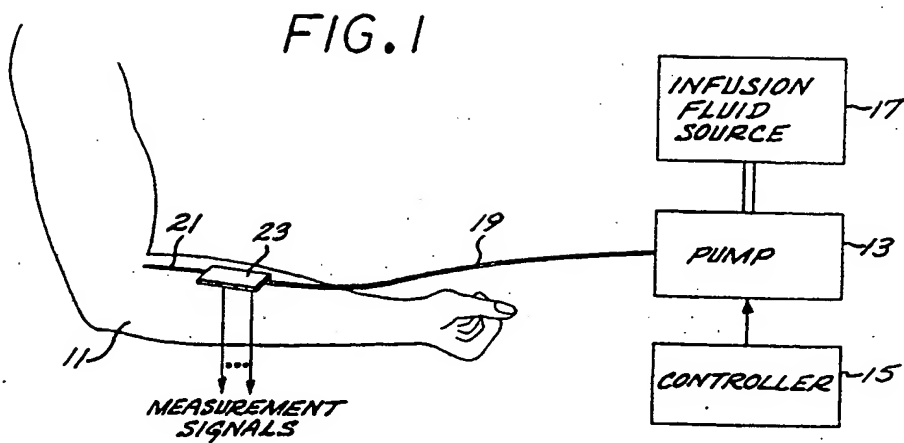


FIG. 2A

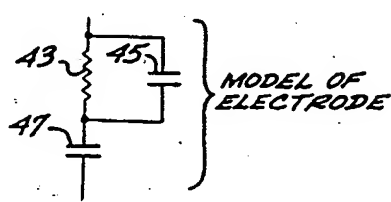


FIG. 2B

# INTERNATIONAL SEARCH REPORT

International Application No

PCT/US 92/09678

| <b>I. CLASSIFICATION OF SUBJECT MATTER</b> (if several classification symbols apply, indicate all) <sup>6</sup><br>According to International Patent Classification (IPC) or to both National Classification and IPC<br>Int.C1. 5 G01N33/49;                      G01N27/26  |  |                                     |   |  |  |  |   |        |   |   |        |   |   |        |
|--|--|-------------------------------------|---|--|--|--|---|--------|---|---|--------|---|---|--------|
| <b>II. FIELDS SEARCHED</b><br><div style="text-align: center; border-top: 1px solid black; border-bottom: 1px solid black; margin: 5px 0;">Minimum Documentation Searched<sup>7</sup></div> <table style="width: 100%; border-collapse: collapse;"> <tr> <th style="width: 30%; border-bottom: 1px solid black;">Classification System</th> <th style="border-bottom: 1px solid black;">Classification Symbols</th> </tr> <tr> <td style="padding: 5px;">Int.C1. 5</td> <td style="padding: 5px;">G01N</td> </tr> </table> <div style="text-align: center; border-top: 1px solid black; border-bottom: 1px solid black; margin: 5px 0;">Documentation Searched other than Minimum Documentation<br/>to the Extent that such Documents are Included in the Fields Searched<sup>8</sup></div>  |  |                                     | Classification System   | Classification Symbols   | Int.C1. 5  | G01N   |   |        |   |   |        |   |   |        |
| Classification System  | Classification Symbols   |                                     |   |  |  |  |   |        |   |   |        |   |   |        |
| Int.C1. 5  | G01N   |                                     |   |  |  |  |   |        |   |   |        |   |   |        |
| <b>III. DOCUMENTS CONSIDERED TO BE RELEVANT<sup>9</sup></b> <table style="width: 100%; border-collapse: collapse;"> <tr> <th style="width: 10%; border-bottom: 1px solid black;">Category<sup>9</sup></th> <th style="border-bottom: 1px solid black;">Citation of Document,<sup>11</sup> with indication, where appropriate, of the relevant passages<sup>12</sup></th> <th style="width: 15%; border-bottom: 1px solid black;">Relevant to Claim No.<sup>13</sup></th> </tr> <tr> <td style="text-align: center; vertical-align: top; padding: 5px;">A</td> <td style="padding: 5px;">           US,A,4 573 968 (PARKER)<br/>           4 March 1986<br/>           see column 2, line 3 - column 5, line 25;<br/>           figures 1-3         </td> <td style="text-align: center; vertical-align: top; padding: 5px;">1,8,13</td> </tr> <tr> <td style="text-align: center; vertical-align: top; padding: 5px;">A</td> <td style="padding: 5px;">           WO,A,8 902 593 (HARMAN)<br/>           23 March 1989<br/>           see page 9, line 12 - page 18, line 8;<br/>           figures 1-7         </td> <td style="text-align: center; vertical-align: top; padding: 5px;">1,8,13</td> </tr> <tr> <td style="text-align: center; vertical-align: top; padding: 5px;">A</td> <td style="padding: 5px;">           US,A,4 818 361 (BURGESS)<br/>           4 April 1989<br/>           see abstract; figures         </td> <td style="text-align: center; vertical-align: top; padding: 5px;">1,8,13</td> </tr> </table> |  |                                     | Category <sup>9</sup>   | Citation of Document, <sup>11</sup> with indication, where appropriate, of the relevant passages <sup>12</sup> | Relevant to Claim No. <sup>13</sup>  | A  | US,A,4 573 968 (PARKER)<br>4 March 1986<br>see column 2, line 3 - column 5, line 25;<br>figures 1-3 | 1,8,13 | A | WO,A,8 902 593 (HARMAN)<br>23 March 1989<br>see page 9, line 12 - page 18, line 8;<br>figures 1-7 | 1,8,13 | A | US,A,4 818 361 (BURGESS)<br>4 April 1989<br>see abstract; figures | 1,8,13 |
| Category <sup>9</sup>  | Citation of Document, <sup>11</sup> with indication, where appropriate, of the relevant passages <sup>12</sup> | Relevant to Claim No. <sup>13</sup> |   |  |  |  |   |        |   |   |        |   |   |        |
| A  | US,A,4 573 968 (PARKER)<br>4 March 1986<br>see column 2, line 3 - column 5, line 25;<br>figures 1-3            | 1,8,13                              |   |  |  |  |   |        |   |   |        |   |   |        |
| A  | WO,A,8 902 593 (HARMAN)<br>23 March 1989<br>see page 9, line 12 - page 18, line 8;<br>figures 1-7              | 1,8,13                              |   |  |  |  |   |        |   |   |        |   |   |        |
| A  | US,A,4 818 361 (BURGESS)<br>4 April 1989<br>see abstract; figures  | 1,8,13                              |   |  |  |  |   |        |   |   |        |   |   |        |
| <div style="display: flex; justify-content: space-between;"> <div style="width: 45%;"> <p><sup>6</sup> Special categories of cited documents: <sup>10</sup></p> <p>"A" document defining the general state of the art which is not considered to be of particular relevance</p> <p>"E" earlier document but published on or after the international filing date</p> <p>"L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)</p> <p>"O" document referring to an oral disclosure, use, exhibition or other means</p> <p>"P" document published prior to the international filing date but later than the priority date claimed</p> </div> <div style="width: 45%;"> <p>"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention</p> <p>"X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step</p> <p>"Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art.</p> <p>"A" document member of the same patent family</p> </div> </div>  |  |                                     |   |  |  |  |   |        |   |   |        |   |   |        |
| <b>IV. CERTIFICATION</b> <table style="width: 100%; border-collapse: collapse;"> <tr> <td style="width: 50%; border-bottom: 1px solid black; padding: 5px;">           Date of the Actual Completion of the International Search<br/> <div style="text-align: center;">03 MARCH 1993</div> </td> <td style="width: 50%; border-bottom: 1px solid black; padding: 5px;">           Date of Mailing of this International Search Report<br/> <div style="text-align: center;">11.03.93</div> </td> </tr> <tr> <td style="border-bottom: 1px solid black; padding: 5px;">           International Searching Authority<br/> <div style="text-align: center;">EUROPEAN PATENT OFFICE</div> </td> <td style="border-bottom: 1px solid black; padding: 5px;">           Signature of Authorized Officer<br/> <div style="text-align: center;">R.A.P. BOSMA</div> </td> </tr> </table>   |  |                                     | Date of the Actual Completion of the International Search<br><div style="text-align: center;">03 MARCH 1993</div> | Date of Mailing of this International Search Report<br><div style="text-align: center;">11.03.93</div>         | International Searching Authority<br><div style="text-align: center;">EUROPEAN PATENT OFFICE</div> | Signature of Authorized Officer<br><div style="text-align: center;">R.A.P. BOSMA</div> |   |        |   |   |        |   |   |        |
| Date of the Actual Completion of the International Search<br><div style="text-align: center;">03 MARCH 1993</div>  | Date of Mailing of this International Search Report<br><div style="text-align: center;">11.03.93</div>         |                                     |   |  |  |  |   |        |   |   |        |   |   |        |
| International Searching Authority<br><div style="text-align: center;">EUROPEAN PATENT OFFICE</div>   | Signature of Authorized Officer<br><div style="text-align: center;">R.A.P. BOSMA</div>                         |                                     |   |  |  |  |   |        |   |   |        |   |   |        |

**ANNEX TO THE INTERNATIONAL SEARCH REPORT  
ON INTERNATIONAL PATENT APPLICATION NO.**

US 9209678  
SA 67244

This annex lists the patent family members relating to the patent documents cited in the above-mentioned international search report.  
The members are as contained in the European Patent Office EDP file on  
The European Patent Office is in no way liable for these particulars which are merely given for the purpose of information. 03/03/93

| Patent document<br>cited in search report | Publication<br>date | Patent family<br>member(s)     | Publication<br>date  |
|---|---------------------|--------------------------------|----------------------|
| US-A-4573968                              | 04-03-86            | None                           |                      |
| WO-A-8902593                              | 23-03-89            | EP-A- 0331696<br>JP-T- 2501162 | 13-09-89<br>19-04-90 |
| US-A-4818361                              | 04-04-89            | None                           |                      |

EPO FORM PWT/9

For more details about this annex : see Official Journal of the European Patent Office, No. 12/82

**This Page Blank (uspto)**

**This Page is Inserted by IFW Indexing and Scanning  
Operations and is not part of the Official Record**

**BEST AVAILABLE IMAGES**

Defective images within this document are accurate representations of the original documents submitted by the applicant.

Defects in the images include but are not limited to the items checked:

- ☒ **BLACK BORDERS**
- ☐ **IMAGE CUT OFF AT TOP, BOTTOM OR SIDES**
- ☐ **FADED TEXT OR DRAWING**
- ☒ **BLURRED OR ILLEGIBLE TEXT OR DRAWING**
- ☐ **SKEWED/SLANTED IMAGES**
- ☐ **COLOR OR BLACK AND WHITE PHOTOGRAPHS**
- ☐ **GRAY SCALE DOCUMENTS**
- ☒ **LINES OR MARKS ON ORIGINAL DOCUMENT**
- ☐ **REFERENCE(S) OR EXHIBIT(S) SUBMITTED ARE POOR QUALITY**
- ☐ **OTHER: \_\_\_\_\_**

**IMAGES ARE BEST AVAILABLE COPY.**

**As rescanning these documents will not correct the image problems checked, please do not report these problems to the IFW Image Problem Mailbox.**

**This Page Blank (uspto)**